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# Distributed Analysis of Hip Implants Using Six National and Regional Registries: Comparing Metal-on-Metal with Metal-on-Highly Cross-Linked Polyethylene Bearings in Cementless Total Hip Arthroplasty in Young Patients

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**Background:** The regulation of medical devices has attracted controversy recently because of problems related to metalon-metal hip implants. There is growing evidence that metal-on-metal implants fail early and cause local and systemic complications. However, the failure associated with metal-on-metal head size is not consistently documented and needs to be communicated to patients and surgeons. The purpose of this study is to compare implant survival of metal on metal with that of metal on highly cross-linked polyethylene.

**Methods:** Using a distributed health data network, primary total hip arthroplasties were identified from six national and regional total joint arthroplasty registries (2001 to 2010). Inclusion criteria were patient age of forty-five to sixty-four years, cementless total hip arthroplasties, primary osteoarthritis diagnosis, and exclusion of the well-known outlier implant ASR (articular surface replacement). The primary outcome was revision for any reason. A meta-analysis of survival probabilities was performed with use of a fixed-effects model. Metal-on-metal implants with a large head size of >36 mm were compared with metal-on-highly cross-linked polyethylene implants.

**Results:** Metal-on-metal implants with a large head size of >36 mm were used in 5172 hips and metal-on-highly cross-linked polyethylene implants were used in 14,372 hips. Metal-on-metal total hip replacements with a large head size of >36 mm had an increased risk of revision compared with metal-on-highly cross-linked polyethylene total hip replacements with more than two years of follow-up, with no difference during the first two years after implantation. The results of the hazard ratios (and 95% confidence intervals) from the multivariable model at various durations of follow-up were 0.95 (0.74 to 1.23) at zero to two years (p = 0.698), 1.42 (1.16 to 1.75) at more than two years to four years (p = 0.001), 1.78 (1.45 to 2.19) at more than four years to six years (p < 0.001), and 2.15 (1.63 to 2.83) at more than six years to seven years (p < 0.001).

**Conclusions:** We conducted a comparison of large-head-size, metal-on-metal implants and metal-on-highly crosslinked polyethylene implants in younger patients with uncemented fixation. We found consistent and strong evidence worldwide that large-head-size, metal-on-metal implants were associated with increased risk of revision after two years compared with metal-on-highly cross-linked polyethylene implants, with the effect becoming more pronounced over time.

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he regulation of medical devices has attracted controversy due to recent problems related to metal-on-metal hip implants<sup>1-5</sup>. There is growing evidence that metal-on-metal implants fail early and cause local and systemic complications<sup>1,6-14</sup>. In a meta-analysis of bearing surfaces using five randomized studies comparing metal-on-metal total hip replacement with metal-on-polyethylene total hip replacement, the investigators found small but significantly better functional results in metal-onpolyethylene total hip replacement<sup>4</sup>. However, head size was not analyzed. Metal-on-metal articulation became popular because metal-on-conventional polyethylene articulation in uncemented cups showed poor results due to wear and osteolysis<sup>15-17</sup>. In vitro, large head sizes improve range of movement and, because of increased jump distance, decrease the risk of dislocation and component impingement<sup>18</sup>. These findings contributed to the increased interest in large-head, metal-on-metal total hip replacement. It has been well established that the ASR (articular surface replacement) metal-on-metal, large-head total hip replacement (DePuy, Leeds, England) had inferior results, and the company withdrew this prosthesis from the market in 2010<sup>1,2,5</sup>.

There has been more uncertainty of the comparative effectiveness of other metal-on-metal total hip replacements<sup>6</sup>. In the Finnish registry study, uncemented, large-head, metal-on-metal total hip replacements had short-term results that were comparable with those of cemented hip implants<sup>6</sup>, contrary to the findings of the National Joint Registry of England and Wales<sup>1</sup> and the Australian Orthopaedic Association National Joint Replacement Registry<sup>3</sup>.

Highly cross-linked polyethylene inserts have shown promising results regarding wear in clinical studies with up to thirteen years of follow-up<sup>19</sup> and in radiostereometric analysis studies with up to ten years of follow-up<sup>20,21</sup>.

The longevity of different bearing surfaces may also depend on the methods of fixation, design, femoral head size, and other operative or implant-related factors. National and regional registries have contributed substantially to detecting inferior implants and techniques<sup>3,22-24</sup>. Single registries might have too few patients or only a limited number of implants; therefore, combining data from several registries could increase power and could broaden inferences to a larger pool of prostheses and to countries around the world<sup>4,25</sup>.

sults from the Fixed-Effects Model*†		
	Hazard Ratio <sup>+</sup>	P Value§
Time (yr)		
One	Reference	_
More than one to two	4.68 (3.86 to 6.12)	<0.001
More than two to three	5.76 (4.39 to 7.55)	<0.001
More than three to four	6.60 (5.02 to 8.69)	<0.001
More than four to five	7.18 (5.43 to 9.49)	<0.001
More than five to six	8.06 (6.07 to 10.72)	<0.001
More than six to seven	8.90 (6.64 to 11.94)	<0.001
More than seven to eight	11.44 (8.13 to 16.11)	<0.001
More than eight to nine	10.78 (7.95 to 15.29)	<0.001
Sex		
Male	Reference	—
Female	1.13 (0.95 to 1.35)	0.174
Age (yr)		
Forty-five to fifty-four	Reference	—
Fifty-five to sixty-four	0.76 (0.62 to 0.93)	0.009
Bearing effects over time#		
Metal on highly cross-linked polyethylene	Reference	
Metal on metal		
At zero to two years	0.95 (0.74 to 1.23)	0.698
At more than two years to four years	1.42 (1.16 to 1.75)	0.001
At more than four years to six years	1.78 (1.45 to 2.19)	<0.001
At more than six years to seven years	2.15 (1.63 to 2.83)	<0.001

\*Fixed registry effects were included in this model (five coefficients), but the results were omitted from this table because a precondition of data sharing was no reporting of between-registry comparisons.  $\dagger$ The value of the estimate and the standard error of the intercept was given as  $-5.257 \pm 0.171$ .  $\ddagger$ The values are given as the hazard ratio, with the 95% CI, which is based on a normal distribution, in parentheses. \$The values are based on a normal distribution. #The effects over time are based on a combination of the main and interaction effects from the model.

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TABLE II Distribution of Non-ASR Metal-on-Metal and Metal-on-Highly Cross-Linked Polyethylene Cementless Total Hip Replacements	
in Patients with Osteoarthritis by Bearing Surface, Head Size, and Sex	

Bearing Surface	Male Patients	No. of Total Hip Replacements*
Metal on highly cross-linked polyethylene	6943 (48.3%)†	14,372 (57.3%)
Metal on metal	6258 (47.4%)†	10,699 (42.7%)
Large head size, >36 mm	3372 (65.2%)‡	5172 (20.6%)
Large head size, 36 mm	1474 (55.2%)‡	2670 (10.6%)
Small head size, ≤32 mm	1412 (49.4%)‡	2857 (11.4%)
Total	13,201 (52.7%)‡	25,071 (100.0%)

\*The values are given as the number of total hip replacements, with the percentage in parentheses. †The values are given as the number of male patients, with the percentages, based on the total number of male patients, in parentheses. +The values are given as the number of male patients, with the row percentage based on the head size of the total hip replacement in parentheses.

The purpose of this study was to compare the implant survival of metal-on-metal total hip replacement with a large head size of >36 mm with that of metal-on-highly cross-linked polyethylene total hip replacement in a homogeneous population of young patients with one fixation type.

#### **Materials and Methods**

Primary total hip arthroplasties were identified from six national and regional total joint arthroplasty registries. To ensure a homogeneous study population, we only included total hip arthroplasties in young patients with an age of forty-five to sixty-four years, uncemented (both acetabulum and femur) total hip replacement, and osteoarthritis as the underlying diagnosis. We excluded the ASR total hip replacement (DePuy) because this implant has been documented as inferior<sup>2,5</sup>. In a previous study, we found metal-on-metal implants with a head size of >36 mm to be associated with an increased risk of revision over time relative to metal-on-metal implants with a head size of <32 mm (results not published). With respect to the 36-mm head size, there was little evidence of a head-size effect (hazard ratio, 1.01 [95% confidence interval (95% CI), 0.31 to 3.27]; p = 0.980), but this estimate varied widely from registry to registry and the random effects variance was 0.326. On the basis of the examination of the deviation of each registry from the mean treatment effect (using empirical best linear unbiased predictions), the U.S. registry (Kaiser Permanente) provided the least evidence of a detrimental effect of the 36-mm head size, which may be attributed to its exclusive use of Pinnacle cups (DePuy), which perform very well at this head size<sup>26</sup>. Fitting a fixed-effects model increased the estimated effect but was still not significant (hazard ratio, 1.40 [95% CI, 0.88 to 2.24]; p = 0.155). In light of these findings, we chose to focus exclusively on metal-on-metal implants with a head size of >36 mm.

The primary outcome was revision for any reason. The definition of revision was the removal, exchange, or addition of any implant parts (including an exchange of inserts and heads only). Metal-on-metal implants with a large head size of >36 mm were compared with metal-on-highly cross-linked polyethylene implants. We analyzed the different highly cross-linked polyethylene head sizes together, as prior analyses have shown that there was no effect of head size on revision in the highly cross-linked polyethylene bearing surface group<sup>27</sup>. The inclusion of patients started on January 1, 2001, and ended on December 31, 2010. The patients were followed until they underwent revision or until the end of the study on December 31, 2010. Death and health plan member terminations were treated as censored cases. A study protocol was developed by investigators, and syntax was sent from the coordinating center located jointly at the Surgical Outcomes & Analysis Department, Kaiser Permanente, San Diego, California, and Weill Cornell Medical College, New York, NY, to each participating registry. In the study, we used a distributed health data network that does not require centralized data storage<sup>4</sup>. Each reg-

istry categorized its implants according to bearing surface, fixation, age, and sex. Each registry identified the highly cross-linked polyethylene inserts and metal-on-metal implants according to the information from the implant companies. Survival probabilities and their standard errors based on a crossclassification of bearing surface, head size, age category, and sex were extracted from each registry and were sent back to the coordinating center where the data were analyzed. No personal identifiable data were sent from the registry, only aggregated data.

#### Statistical Analysis

A multivariate meta-analysis was performed using linear mixed models comparing metal-on-metal total hip replacement with a large head size of >36 mm with metal-on-highly cross-linked polyethylene total hip replacements of all head sizes, with survival probability as the unit of analysis<sup>28</sup>. The models estimate the residual covariances using the precise method of Dear<sup>29</sup> and implement a transformation<sup>30,31</sup> to ensure that the models can be fit with existing software (SAS version 9.2; SAS Institute, Cary, North Carolina). Survival probabilities and their standard errors were extracted from each registry for each unique combination of the covariates listed above at each distinct event time, and each unique combination was grouped into yearly time intervals, with only the earliest observation in that interval retained. We fit two models, one that treated registry as a set of fixed effects and another that treated registry as random effect(s). Although the random-effects model offers some inferential advantage<sup>32,33</sup>, with few observational data or registries, the estimated betweenregistry variation in the random-effects model can be quite inaccurate. Further, the absence of randomization for bearing and head-size groups could lead to confounding due to registry-level effects, which is addressed by the fixed-effects model but not by the random-effects model<sup>34,35</sup>. Therefore, preference would be given to interpretation of the fixed-effects model, particularly if the parameter estimates are substantially different in the fixed-effects model compared with the random-effects model<sup>34,35</sup>. Hence, we present the results of the fixed-effects model in Table I and include the results of the random-effects model in the Appendix. SAS version 9.2 (SAS Institute) was used for all analyses.

#### Results

The study cohort was based on six national and regional registries and consisted of 19,544 cementless total hip arthroplasties, in which metal-on-metal implants with a large head size of >36 mm were used in 5172 hips (26.5%) and metal-on-highly cross-linked polyethylene implants were used in 14,372 hips (73.5%) (Table II). Six registries contributed data to the study: the Australian Orthopaedic Association National Joint Replacement Registry (n = 12,482), the Kaiser The Journal of Bone & Joint Surgery · JBJS.org Volume 96-A · Supplement 1(E) · 2014 DISTRIBUTED ANALYSIS OF HIP IMPLANTS USING SIX NATIONAL AND REGIONAL REGISTRIES

			Registr	/*		
	United States (Kaiser Permanente)	Australia	ltaly (Emilia-Romagna Region)	United States (HealthEast)	Norway	Spain (Catalan Region)
Metal on highly cross-linked polyethylene, <32-mm head size						
Age						
Forty-five to fifty-four years	194 (23.0%)	1109 (24.3%)	26 (10.4%)	56 (32.9%)	33 (22.1%)	30 (30.9%
Fifty-five to sixty-four years	648 (77.0%)	3462 (75.7%)	224 (89.6%)	114 (67.1%)	116 (77.9%)	67 (69.1%
Sex						
Male	275 (32.7%)	2110 (46.2%)	121 (48.4%)	63 (37.1%)	51 (34.2%)	61 (62.9%
Female	567 (67.3%)	2461 (53.8%)	129 (51.6%)	107 (62.9%)	98 (65.8%)	36 (37.1%
Metal on highly cross-linked polyethylene, 32-mm head size						
Age						
Forty-five to fifty-four years	347 (18.6%)	554 (21.2%)	1 (12.5%)	23 (30.3%)	3 (21.4%)	14 (25.5%
Fifty-five to sixty-four years	1516 (81.4%)	2062 (78.8%)	7 (87.5%)	53 (69.7%)	11 (78.6%)	41 (74.5%
Sex						
Male	723 (38.8%)	1253 (47.9%)	1 (12.5%)	42 (55.3%)	6 (42.9%)	28 (50.9%
Female	1140 (61.2%)	1363 (52.1%)	7 (87.5%)	34 (44.7%)	8 (57.1%)	27 (49.1%
Metal on highly cross-linked polyethylene, >32-mm head size						
Age						
Forty-five to fifty-four years	352 (19.3%)	367 (22.2%)	6 (22.2%)	15 (14.2%)	2 (40.0%)	7 (14.3%
Fifty-five to sixty-four years	1471 (80.7%)	1284 (77.8%)	21 (77.8%)	91 (85.8%)	3 (60.0%)	42 (85.7%
Sex						
Male	1020 (56.0%)	1060 (64.2%)	23 (85.2%)	71 (67.0%)	5 (100.0%)	30 (61.2%
Female	803 (44.0%)	591 (35.8%)	4 (14.8%)	35 (33.0%)	0 (0.0%)	19 (38.8%
Non-ASR metal on metal, >36-mm head size						
Age						
Forty-five to fifty-four years	326 (37.1%)	1228 (33.7%)	126 (29.0%)	27 (31.0%)	12 (52.2%)	30 (28.3%
Fifty-five to sixty-four years	552 (62.9%)	2416 (66.3%)	308 (71.0%)	60 (69.0%)	11 (47.8%)	76 (71.7%
Sex						
Male	629 (71.6%)	2261 (62.0%)	296 (68.2%)	80 (92.0%)	19 (82.6%)	87 (82.1%
Female	249 (28.4%)	1383 (38.0%)	138 (31.8%)	7 (8.0%)	4 (17.4%)	19 (17.9%

Permanente Total Joint Registry (United States) (n = 5406), the HealthEast Joint Replacement Registry (United States) (n = 439), the Emilia-Romagna Joint Registry R.I.P.O. (Registro dell'implantologia Protesica Ortopedica [Registry of the Orthopaedic Prosthetic Implants]) (Italy) (n = 719), the Norwegian Arthroplasty Register (n = 191), and the Catalan Arthroplasty Register (Spain) (n = 307). The distribution of bearing surfaces, sex, and age in each registry is shown in Table III.

The results of a fixed-effects model comparing metalon-metal total hip replacements with a head size of >36 mm with metal-on-highly cross-linked polyethylene total hip replacements are presented in Table I, which consists of treating registry membership as a set of fixed effects. The advantage of this approach is that it controls for all registry-level confounding. The results of a random-effects model are presented in the Appendix with details of how these models were selected. Most relevant in Table I are the entries for bearing surface effects over time, showing that there is no evidence of a difference between the bearings at zero to two years (hazard ratio, 0.95 [95% CI, 0.74 to 1.23]; p = 0.698), but there is a greater The Journal of Bone & Joint Surgery • JBJS.org Volume 96-A • Supplement 1(E) • 2014 DISTRIBUTED ANALYSIS OF HIP IMPLANTS USING SIX NATIONAL AND REGIONAL REGISTRIES



#### Fig. 1

Model-predicted survival of the results of Table I comparing metal-on-metal implants with a head size of >36 mm with metal-on-highly cross-linked polyethylene (HXPLE) implants of all head sizes. The x-axis values of 1 to 9 correspond to the interval years of zero to one year to more than eight years to nine years.

risk of metal-on-metal failures appearing thereafter at more than two years to four years (hazard ratio, 1.42 [95% CI, 1.16 to 1.75]; p = 0.001), at more than four years to six years (hazard ratio, 1.78 [95% CI, 1.45 to 2.19]; p < 0.001), and at more than six years to seven years (hazard ratio, 2.15 [95% CI, 1.63 to 2.83]; p < 0.001). These effects were similar for the random-effects model. Figure 1 displays the model-predicted survival for each head-size group from the fixed-effects model.

## **Discussion**

With the exclusion of the ASR implant, we provided a comprehensive analysis of the metal-on-metal total hip replacement implant outcomes in younger osteoarthritic patients using uncemented fixation. Metal-on-metal implants with a large head size of >36 mm were associated with a higher risk of revision when compared with metal-on-highly cross-linked polyethylene implants. There was no difference in the first two years, but revision risk increased thereafter to greater than a twofold risk at a follow-up of six to seven years.

# Evidence from the Literature

With increasing diameter of the head, the wear of large-head, metal-on-metal implants decreases, but the taper damage increases<sup>2</sup>. The resulting wear causes high metal ion levels and pseudotumors<sup>7,11,12</sup>. It also explains why, when compared with small-head resurfacing hip implants, large-head resurfacing metal-on-metal hip implants have less risk of revision<sup>24,26</sup> and

large-head metal-on-metal total hip replacements have more risk of revision<sup>1,26</sup>. Our study confirms these findings. In a meta-analysis of four randomized studies<sup>36</sup> comparing metalon-metal and metal-on-polyethylene hip replacements, Voleti et al. found no difference in functional outcome, but a 3.37 times higher complication rate in the metal-on-metal total hip replacement group. In a meta-analysis of five studies on metalon-metal total hip replacements compared with metal-onpolyethylene total hip replacements, Sedrakyan and coworkers found a small but significantly lower functional score using the Harris hip score in metal-on-metal total hip replacement<sup>4</sup>. However, head size was not analyzed in that meta-analysis, and three of the included studies compared 28-mm metal-on-metal components with 28-mm metal-on-polyethylene components. In that same study, three national registries reported more revision in metal-on-metal total hip replacement compared with metal-on-polyethylene total hip replacement. In a large study from the National Joint Registry of England and Wales<sup>24</sup>, one type of stem (the Corail stem) used in total hip arthroplasty was studied, and risk factors for revision were investigated. Those investigators found that metal-on-metal total hip replacement had a hazard ratio of 1.93 at a follow-up duration of 7.5 years compared with metal-on-polyethylene replacement, which is in accordance with our findings.

The brand of metal-on-metal total hip replacement is important. The Finnish Arthroplasty Register found that the cementless Spotorno (CLS) stem combined with the Durom The Journal of Bone & Joint Surgery • JBJS.org Volume 96-A • Supplement 1(E) • 2014 DISTRIBUTED ANALYSIS OF HIP IMPLANTS USING SIX NATIONAL AND REGIONAL REGISTRIES

cup had a 2.9 times increased revision risk compared with the cementless Synergy stem combined with the Birmingham Hip Resurfacing (BHR) cup<sup>6</sup>. The Finnish study could not demonstrate a difference in revision risk between cementless metalon-metal total hip replacement compared with cemented metal-on-polyethylene total hip replacement<sup>6</sup> with a maximum seven-year follow-up. Our study compared only cementless total hip replacement, which makes it less prone to confounding by indication. However, in a recent study from a Finnish hospital<sup>6</sup>, 54% of eighty patients followed for a mean duration of six years had definite, probable, or possible adverse reaction to metal debris, but only three of the patients had undergone revision. In the selection model using random head size outlined in the Appendix, we did not find a head-size effect comparing metal on metal at 36 mm and at ≤32 mm, but there was substantial variation between registries. However, we advocate caution in the use of small head size in metal-on-metal implants. A randomized study of 397 hips from Norway comparing small-head (28 mm) Metasul metal-on-metal implants, small-head metal-on-conventional polyethylene implants, and ceramic-on-conventional polyethylene implants with seven years of follow-up showed no advantage of the metal-on-metal bearing with a higher revision rate and greater incidence of radiolucent lines in the metal-onmetal group than with the two other articulations<sup>37</sup>.

Several governmental medical regulatory agencies, including the Medicines and Healthcare Products Regulatory Agency, have issued warnings and have recommended regular follow-up for metal-on-metal total hip replacements and hip resurfacing, and the number of metal-on-metal total hip replacements has decreased substantially. Our study should dispel uncertainty related to large-head-size, metal-on-metal total hip replacements. The increased risk of large-head-size, metalon-metal total hip replacements needs to be communicated to regulators, clinicians, and patients.

# Strengths and Limitations

The strengths of this study were the homogeneous study population of young patients with only uncemented implants with osteoarthritis as diagnosis, the comparison with highly crosslinked polyethylene (and not a mixture of standard polyethylene and highly cross-linked polyethylene), and the use of data from six national and regional registries. The external validity of the study can therefore be regarded as good. Another strength was the number of implants studied, with 5172 metal-on-metal total hip replacements compared with 14,372 metal-on-highly crosslinked polyethylene hip implants in younger age groups, thus being, to our knowledge, the largest registry-based study for this age group reported. A limitation of the study was that the maximum follow-up was short to mid-term (up to nine years). Currently, the harmonization of implant databases across registries has not been completed and there is no comparison of implant designs across countries. While the average follow-up rate in the registries is >90%, there are limitations of observational data collected by registries. Therefore, such data would not be sufficient to support a marketing application in the U.S. Larger registries with longer follow-up would likely have a stronger

influence on estimates, and differential follow-up time and implant brands used in the registries also could have influenced the results.

The case of confidentiality of the patients from each registry was not an issue because we used a standardized syntax to extract aggregated data from each registry. This approach did not necessitate institutional ethical board review as each registry's legal approval could be used. The method is less flexible because changes in the syntax require new analysis to be conducted by each registry, but it protects registry data and participation. Another approach used in the Nordic Arthroplasty Register Association (NARA)<sup>25</sup> might be more flexible as it creates one file for analysis with anonymous data on which researchers can do repeated analysis, but it requires a higher level of agreement by the registries and a continuous update of the main analytic file as new data are accumulating. A limitation of our study was that it was based on a minimal data set, limited by the data available from each registry. Currently, the harmonization of implant databases across registries is under development, and in the future we can validate the implants in each group. Larger registries with longer follow-up would likely have had a stronger influence on estimates, and differential follow-up time and implant brands used in the registries also could have influenced the results.

### Future Research

The effect of the different head sizes in large-head, metal-onmetal total hip replacements will be studied in the future, as well as various bearing surfaces in individual age groups, including a number of brands of highly cross-linked polyethylene. An important step in international registry studies will be the harmonization of different implants in a standardized implant database across registries and categorization of implants. Inclusion of new registries in the project is ongoing, providing a larger number of patients with longer durations of follow-up.

In conclusion, we demonstrated the potential of the international research network and conducted a robust study using advanced harmonized distributed analyses of six national and regional joint replacement registries. We provided a comprehensive analysis of the metal-on-metal implant outcomes in younger patients using uncemented fixation, with a well-known outlier implant excluded. We found consistent and strong evidence worldwide that large-head-size, metal-on-metal implants were associated with a higher risk of revision when compared with the metal-on-highly cross-linked polyethylene bearing. Higher revision occurs later in time rather than early after surgery.

# **Appendix—Details of the Model Fitting** Data Inclusion

 $\mathbf{F}$  or the models described here, we chose to retain observations with standard errors of <0.025, given simulations indicating increased bias, root mean squared error, and poorer coverage when observations with large degrees of imprecision (resulting from sparse data for certain covariate combinations) are retained. This particular threshold was based on both the simulation results and a sensitivity analysis comparing the effect on model parameters when different levels of restriction (0.05, 0.025, and 0.0125) are applied. The Journal of Bone & Joint Surgery · jbjs.org Volume 96-A · Supplement 1(E) · 2014 DISTRIBUTED ANALYSIS OF HIP IMPLANTS USING SIX NATIONAL AND REGIONAL REGISTRIES

	Hazard Ratio†	P Value
Time (yr)		
Zero to one	Reference	_
More than one to two	4.446 (3.415 to 5.789)	<0.001
More than two to three	5.474 (4.188 to 7.155)	<0.001
More than three to four	6.272 (4.786 to 8.218)	<0.001
More than four to five	6.826 (5.189 to 8.979)	<0.001
More than five to six	7.666 (5.798 to 10.137)	<0.001
More than six to seven	8.449 (6.337 to 11.265)	<0.001
More than seven to eight	10.856 (7.766 to 15.175)	<0.001
More than eight to nine	10.232 (7.256 to 14.429)	<0.001
Sex		
Male	Reference	—
Female	1.127 (0.943 to 1.349)	0.187
Age (yr)		
Forty-five to fifty-four	Reference	_
Fifty-five to sixty-four	0.781 (0.637 to 0.957)	0.018
Bearing effects over time*		
Metal on highly cross-linked polyethylene§	Reference	_
Metal on metal#		
At zero to two years	0.964 (0.747 to 1.243)	0.773
At more than two to four years	1.424 (0.993 to 2.043)	0.053
At more than four to six years	1.814 (1.478 to 2.227)	< 0.002
At more than six to seven years	2.207 (1.670 to 2.917)	<0.00'

\*The estimate and the standard error were  $-5.238 \pm 0.165$  for the intercept and  $0.003 \pm 0.059$  for the random effect of a metal-on-metal implant at a time of more than two years to four years. The random effect is based on the coefficient corresponding to the interaction effect for this time interval. Results are based on an iterative solution that updates the residual covariances until convergence. The random-effects model is estimated using the restricted maximum likelihood. Our simulations indicate that an optimal strategy for confidence interval construction in the presence of random effects is to use  $t_{K-1}$  for fixed parameters with corresponding random effects and  $t_{n-p}$  otherwise (where K-1 and n-p indicate the degrees of freedom for the t distribution, n is the number of observations, p is the number of fixed effects, and k is the number of registries). †The values are given as the hazard ratio, with the 95% CI in parentheses. †The effects over time are based on a combination of the main and interaction effects and p values; all others use  $t_{n-p}$ . §Metal-on-highly cross-linked polyethylene bearings are all head sizes. #Metal-on-metal bearings have head sizes of >36 mm and exclude ASR implants.

## Model Selection

The fixed-effects model was based on the random-effects model selected. Details related to the selection of the random-effects model are provided below.

Metal-on-Metal Implants with Head Sizes of 36 mm and  $\leq$ 32 mm Prior to making comparisons of metal-on-metal implants with metal-on-highly cross-linked polyethylene implants, we conducted analyses of metal-on-metal implants (excluding ASR implants) with a head size of 36 mm compared with a head size of  $\leq$ 32 mm. We fitted a model with an intercept, head size, age, sex, piecewise constant function of time, random head-size effect, and residual variance fixed at 1. For the comparison of metalon-metal head sizes of 36 mm and  $\leq$ 32 mm, the interaction terms were based on the following intervals of time in years: zero to two years, more than two years to four years, and more

than four years to six years. There was no evidence of a significant interaction in this model ( $\chi^2(2) = 0.56$ ; p = 0.754), and these terms were subsequently removed. From this model, there was no evidence of a fixed head-size effect, with a  $\beta$  (and a standard error) of 0.011  $\pm$  0.388 (p = 0.977), but there was substantial between-registry variation across head size, with a  $\sigma^2_{head size}$  (and standard error) of 0.326 ± 0.375. An examination of the empirical best linear unbiased predictions (estimate of the deviation of each registry from the average head-size effect) indicates that the registry for the United States (Kaiser Permanente) produced the least evidence for the harmful effect of a 36-mm head size at -0.61, followed by those for Italy (Emilia-Romagna) at 0.01, Australia at 0.30, and again the United States (HealthEast) at 0.31. Therefore, we focus on the >36-mm metal-on-metal head sizes for this analysis.

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Metal-on-Metal Implants with a Head Size of >36-mm Compared with Metal-on-Highly Cross-Linked Polyethylene Implants at All Head Sizes

Including an interaction is motivated by findings that the risk for failure increases with large head size, metal-on-metal implants over time (see Table IV). The interaction terms were based on intervals of time: zero to two years, more than two years to four years, more than four years to six years, and more than six years to seven years. The intervals of time were constructed in this way to improve precision in estimation relative to the use of single-year intervals. The last interval contains only one year because there is no survival information for the metal-on-metal implants in this data set after seven years. There was improvement in model fit with the inclusion of the interaction terms  $\chi^2(3) = 33.70$  and p < 0.001. Lastly, we considered the addition of random effects for the bearing effect for each of these time intervals. These effects were estimated to be near zero ( $<1.0 \times 10^{-10}$ ) or would not converge for all but the interaction term corresponding to the interval of time at more than two years to four years. The addition of this random effect led to a nearzero random-effects variance estimate for the intercept; as a result, the latter effect was subsequently removed from the model.

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#### References

**1.** Smith AJ, Dieppe P, Vernon K, Porter M, Blom AW; National Joint Registry of England and Wales. Failure rates of stemmed metal-on-metal hip replacements: analysis of data from the National Joint Registry of England and Wales. Lancet. 2012 Mar 31;379(9822):1199-204. Epub 2012 Mar 13.

**2.** Langton DJ, Jameson SS, Joyce TJ, Gandhi JN, Sidaginamale R, Mereddy P, Lord J, Nargol AV. Accelerating failure rate of the ASR total hip replacement. J Bone Joint Surg Br. 2011 Aug;93(8):1011-6.

**3.** Graves SE, Rothwell A, Tucker K, Jacobs JJ, Sedrakyan A. A multinational assessment of metal-on-metal bearings in hip replacement. J Bone Joint Surg Am. 2011 Dec 21;93(Suppl 3):43-7.

**4.** Sedrakyan A, Paxton EW, Phillips C, Namba R, Funahashi T, Barber T, Sculco T, Padgett D, Wright T, Marinac-Dabic D. The International Consortium of Orthopaedic Registries: overview and summary. J Bone Joint Surg Am. 2011 Dec 21; 93(Suppl 3):1-12.

 de Steiger RN, Hang JR, Miller LN, Graves SE, Davidson DC. Five-year results of the ASR XL Acetabular System and the ASR Hip Resurfacing System: an analysis from the Australian Orthopaedic Association National Joint Replacement Registry. J Bone Joint Surg Am. 2011 Dec 21;93(24):2287-93.

6. Mokka J, Junnila M, Seppänen M, Virolainen P, Pölönen T, Vahlberg T, Mattila K, Tuominen EK, Rantakokko J, Aärimaa V, Kukkonen J, Mäkelä KT. Adverse reaction to metal debris after ReCap-M2A-Magnum large-diameter-head metal-on-metal total hip arthroplasty. Acta Orthop. 2013 Dec;84(6):549-54. Epub 2013 Oct 31.

7. Wilkinson JM. Metal-on-metal hip prostheses: where are we now? BMJ.

2012;345:e7792. Epub 2012 Nov 16.

8. Prentice JR, Clark MJ, Hoggard N, Morton AC, Tooth C, Paley MN, Stockley I, Hadjivassiliou M, Wilkinson JM. Metal-on-metal hip prostheses and systemic health:

a cross-sectional association study 8 years after implantation. PLoS One. 2013;8 (6):e66186. Epub 2013 Jun 10.

**9.** Jacobs JJ, Wimmer MA. An important contribution to our understanding of the performance of the current generation of metal-on-metal hip replacements. J Bone Joint Surg Am. 2013 Apr 17;95(8):e53.

**10.** Liao Y, Hoffman E, Wimmer M, Fischer A, Jacobs J, Marks L. CoCrMo metal-on-metal hip replacements. Phys Chem Chem Phys. 2013 Jan 21;15(3): 746-56.

**11.** Hart AJ, Quinn PD, Lali F, Sampson B, Skinner JA, Powell JJ, Nolan J, Tucker K, Donell S, Flanagan A, Mosselmans JF. Cobalt from metal-on-metal hip replacements may be the clinically relevant active agent responsible for periprosthetic tissue reactions. Acta Biomater. 2012 Oct;8(10):3865-73. Epub 2012 Jun 9.

**12.** Hart AJ, Satchithananda K, Liddle AD, Sabah SA, McRobbie D, Henckel J, Cobb JP, Skinner JA, Mitchell AW. Pseudotumors in association with well-functioning metalon-metal hip prostheses: a case-control study using three-dimensional computed tomography and magnetic resonance imaging. J Bone Joint Surg Am. 2012 Feb 15;94(4):317-25.

**13.** Mann BS, Whittingham-Jones PM, Shaerf DA, Nawaz ZS, Harvie P, Hart AJ, Skinner JA. Metal-on-metal bearings, inflammatory pseudotumours and their neurological manifestations. Hip Int. 2012 Mar-Apr;22(2):129-36.

**14.** Ardaugh BM, Graves SE, Redberg RF. The 510(k) ancestry of a metal-on-metal hip implant. N Engl J Med. 2013 Jan 10;368(2):97-100.

**15.** Havelin LI, Espehaug B, Engesaeter LB. The performance of two hydroxyapatitecoated acetabular cups compared with Charnley cups. From the Norwegian Arthroplasty Register. J Bone Joint Surg Br. 2002 Aug;84(6):839-45. **16.** Hallan G, Dybvik E, Furnes O, Havelin LI. Metal-backed acetabular components with conventional polyethylene: a review of 9113 primary components with a followup of 20 years. J Bone Joint Surg Br. 2010 Feb;92(2):196-201.

**17.** Min BW, Song KS, Kang CH, Won YY, Koo KH. Polyethylene liner failure in second-generation Harris-Galante acetabular components. J Arthroplasty. 2005 Sep;20(6):717-22.

**18.** Burroughs BR, Hallstrom B, Golladay GJ, Hoeffel D, Harris WH. Range of motion and stability in total hip arthroplasty with 28-, 32-, 38-, and 44-mm femoral head sizes. J Arthroplasty. 2005 Jan;20(1):11-9.

**19.** Bragdon CR, Doerner M, Martell J, Jarrett B, Palm H, Malchau H; Multicenter Study Group. The 2012 John Chamley Award: Clinical multicenter studies of the wear performance of highly crosslinked remelted polyethylene in THA. Clin Orthop Relat Res. 2013 Feb;471(2):393-402.

**20.** Digas G, Kärrholm J, Thanner J, Herberts P. 5-year experience of highly crosslinked polyethylene in cemented and uncemented sockets: two randomized studies using radiostereometric analysis. Acta Orthop. 2007 Dec;78(6):746-54.

**21.** Röhrl SM, Nivbrant B, Nilsson KG. No adverse effects of submelt-annealed highly crosslinked polyethylene in cemented cups: an RSA study of 8 patients 10 years after surgery. Acta Orthop. 2012 Apr;83(2):148-52. Epub 2012 Jan 17.

**22.** Havelin LI, Espehaug B, Vollset SE, Engesaeter LB. Early aseptic loosening of uncemented femoral components in primary total hip replacement. A review based on the Norwegian Arthroplasty Register. J Bone Joint Surg Br. 1995 Jan; 77(1):11-7.

**23.** Havelin LI, Espehaug B, Vollset SE, Engesaeter LB. The effect of the type of cement on early revision of Charnley total hip prostheses. A review of eight thousand five hundred and seventy-nine primary arthroplasties from the Norwegian Arthroplasty Register. J Bone Joint Surg Am. 1995 Oct;77(10):1543-50.

**24.** Jameson SS, Baker PN, Mason J, Rymaszewska M, Gregg PJ, Deehan DJ, Reed MR. Independent predictors of failure up to 7.5 years after 35 386 single-brand cementless total hip replacements: a retrospective cohort study using National Joint Registry data. Bone Joint J. 2013 Jun;95(6):747-57.

25. Havelin LI, Fenstad AM, Salomonsson R, Mehnert F, Furnes O, Overgaard S, Pedersen AB, Herberts P, Kärrholm J, Garellick G, The Nordic Arthroplasty Register

DISTRIBUTED ANALYSIS OF HIP IMPLANTS USING SIX NATIONAL AND REGIONAL REGISTRIES

Association: a unique collaboration between 3 national hip arthroplasty registries with 280,201 THRs. Acta Orthop. 2009 Aug;80(4):393-401.

**26.** Graves S, Davidson D, de Steiger R, Tomkins A. Australian Orthopaedic Association National Joint Replacement Registry. Annual Report. 2012. https://aoanjrr.dmac.adelaide.edu.au/documents/10180/60142/Annual% 20Report%202012?version=1.3&t=1361226543157. Accessed 2014 May 8.

**27.** Allepuz A, Havelin L, Barber T, Sedrakyan A, Graves S, Bordini B, Hoeffel D, Cafri G, Paxton E. Effect of femoral head size on metal-on-HXLPE hip arthroplasty outcome in a combined analysis of six national and regional registries. J Bone Joint Surg Am. 2014 Dec 17;96(Suppl 1):12-8.

**28.** Arends LR, Hunink MG, Stijnen T. Meta-analysis of summary survival curve data. Stat Med. 2008 Sep 30;27(22):4381-96.

**29.** Dear KB. Iterative generalized least squares for meta-analysis of survival data at multiple times. Biometrics. **1994** Dec;50(4):989-1002.

**30.** Kutner MH, Nachtsheim CJ, Neter J, Li W. Applied linear statistical models. 5th ed. Boston, MA: McGraw-Hill/Irwin; 2005.

**31.** Kalaian HA, Raudenbush SW. A multivariate mixed linear model for metaanalysis. Psychol Methods. 1996;1(3):227-35.

**32.** DerSimonian R, Laird N. Meta-analysis in clinical trials. Control Clin Trials. 1986 Sep;7(3):177-88.

**33.** Hedges LV, Vevea JL. Fixed- and random-effects models in meta-analysis. Psychol Methods. 1998;3(4):486-504.

**34.** Localio AR, Berlin JA, Ten Have TR, Kimmel SE. Adjustments for center in multicenter studies: an overview. Ann Intern Med. 2001 Jul 17;135(2): 112-23.

35. Allison PD. Fixed effects regression models. Thousand Oaks, CA: Sage; 2009.
36. Voleti PB, Baldwin KD, Lee GC. Metal-on-metal vs conventional total hip arthroplasty: a systematic review and meta-analysis of randomized controlled trials. J Arthroplasty. 2012 Dec;27(10):1844-9. Epub 2012 Jul 6.

**37.** Bjorgul K, Novicoff WN, Andersen ST, Ahlund OR, Bunes A, Wiig M, Brevig K. High rate of revision and a high incidence of radiolucent lines around Metasul metalon-metal total hip replacements: results from a randomised controlled trial of three bearings after seven years. Bone Joint J. 2013 Jul;95(7):881-6.